Joint Encoding of Auditory Timing and Location in Visual Cortex

John Plass
EunSeon Ahn
Vernon L. Towle
William C. Stacey
Vibhangini S. Wasade

Henry Ford Health System, VWASADE1@hfhs.org

See next page for additional authors

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Authors
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Joint Encoding of Auditory Timing and Location in Visual Cortex

John Plass\textsuperscript{1}, EunSeon Ahn\textsuperscript{1}, Vernon L. Towle\textsuperscript{2}, William C. Stacey\textsuperscript{1}, Vibhangini S. Wasade\textsuperscript{3}, James Tao\textsuperscript{2}, Shasha Wu\textsuperscript{2}, Naoum P. Issa\textsuperscript{2}, and David Brang\textsuperscript{1}

Abstract

Co-occurring sounds can facilitate perception of spatially and temporally correspondent visual events. Separate lines of research have identified two putatively distinct neural mechanisms underlying two types of crossmodal facilitations: Whereas crossmodal phase resetting is thought to underlie enhancements based on temporal correspondences, lateralized occipital evoked potentials (ERPs) are thought to reflect enhancements based on spatial correspondences. Here, we sought to clarify the relationship between these two effects to assess whether they reflect two distinct mechanisms or, rather, two facets of the same underlying process. To identify the neural generators of each effect, we examined crossmodal responses to lateralized sounds in visually responsive cortex of 22 patients using electrocorticographic recordings. Auditory-driven phase reset and ERP responses in visual cortex displayed similar topography, revealing significant activity in pericalcarine, inferior occipital–temporal, and posterior parietal cortex, with maximal activity in lateral occipitotemporal cortex (potentially V5/hMT+). Laterality effects showed similar but less widespread topography. To test whether lateralized and nonlateralized components of crossmodal ERPs emerged from common or distinct neural generators, we compared responses throughout visual cortex. Visual electrodes responded to both contralateral and ipsilateral sounds with a contralateral bias, suggesting that previously observed laterality effects do not emerge from a distinct neural generator but rather reflect laterality-biased responses in the same neural populations that produce phase-resetting responses. These results suggest that crossmodal phase reset and ERP responses previously found to reflect spatial and temporal facilitation in visual cortex may reflect the same underlying mechanism. We propose a new unified model to account for these and previous results.

INTRODUCTION

Co-occurring sounds can facilitate the perception of spatially or temporally correspondent visual events. Salient lateralized sounds can enhance the detection and discrimination of colocated visual targets (Lu et al., 2009; Driver & Spence, 2004; McDonald, Teder-Sälejärvi, & Hillyard, 2000; Spence & Driver, 1997), whereas spatially uninformative sounds can enhance the detection, discrimination, and perceived temporal dynamics of co-occurring visual stimuli (Chen, Huang, Yeh, & Spence, 2011; Fiebelkorn, Foxe, Butler, Mercier, et al., 2011; Jaekl & Soto-Faraco, 2010; Noesselt et al., 2010; Shams, Kamitani, & Shimojo, 2002; Shipley, 1964). However, it is currently unclear whether audiovisual interactions based on spatial and temporal correspondences are subserved by the same or distinct neural mechanisms for crossmodal enhancement.

Separate lines of research have previously identified two putatively distinct mechanisms thought to underlie crossmodal facilitations based on each type of audiovisual correspondence. On the one hand, crossmodal phase resetting (i.e., auditory resetting of oscillations in visual cortex) is thought to facilitate visual perception for temporally correspondent stimuli by placing visual cortex in a high-excitability state before visual signals arrive (Mercier et al., 2013; Romei, Gross, & Thut, 2012; Naue et al., 2011; Lakatos et al., 2009; for a review, see Thorne & Debener, 2014). Because this mechanism produces transient increases in visual cortical sensitivity that are time-locked to auditory events, it can be seen as primarily producing crossmodal enhancements based on temporal correspondences between auditory and visual stimuli.

On the other hand, interhemispheric laterality differences in occipital ERPs produced by spatialized sounds are thought to reflect hemisphere-specific crossmodal excitation (or suppression) of activity in visual cortex (Campus, Sandini, Morrone, & Gori, 2017; Matusz, Retsa, & Murray, 2016; Brang et al., 2015; Feng, Störmer, Martinez, McDonald, & Hillyard, 2014; McDonald, Störmer, Martinez, Feng, & Hillyard, 2013; for a review, see Hillyard, Störmer, Feng, Martinez, & McDonald, 2016). By modulating visual activity in a hemisphere-specific manner, these effects are thought to selectively enhance the neural encoding of spatially correspondent visual stimuli, potentially reflecting a mechanism for the crossmodal...
orienting of exogenous visuospatial attention (Hillyard et al., 2016).

Differences in the apparent timing and neural topography of the effects associated with each putative mechanism have led researchers to study and interpret them primarily as independent processes. Whereas activity associated with crossmodal phase resetting is typically observed 20–150 msec after sound onset (Mercier et al., 2013; Romei et al., 2012; Naue et al., 2011; Lakatos et al., 2009), lateralized ERP differences during this period are typically attributed to auditory neural generators, with only later (150–400 msec) laterality effects typically being localized to visual cortex (Matusz et al., 2016; Feng et al., 2014; McDonald et al., 2013). Moreover, crossmodal phase resetting is typically observed in or localized to low-level visual cortex, including primary visual cortex (Naue et al., 2011; Lakatos et al., 2009), whereas lateralized ERP differences are typically localized to ventral–lateral occipital regions associated with higher order visual processing (Matusz et al., 2016; Feng et al., 2014; McDonald et al., 2013).

However, additional findings call into question a strict neural dissociation between these two types of facilitation. First, whereas most scalp-recorded EEG studies tend to show the clearest laterality effects at later time points, at least one has found robust lateralized occipital responses as early as 50–100 msec after sound onset, specifically when the locations of auditory stimuli were task relevant (Campus et al., 2017). Early occipital laterality differences have also been observed in other studies using scalp-recorded EEG (e.g., McDonald et al., 2013) but have been attributed to lateralized sources in auditory cortex on the basis of source localization analyses. However, given the limited spatial resolution of scalp-recorded EEG and potential weakness of EEG source localization procedures (Bradley, Yao, Dewald, & Richter, 2016), it is possible that these early laterality differences are at least partially attributable to lateralized responses in visual cortex. Second, source localizations of late-lateralized responses have not always unambiguously identified ventral–lateral occipital sources, with some source estimates including more medial sources potentially corresponding to low-level visual regions implicated in studies of phase resetting (Matusz et al., 2016; Feng et al., 2014). Finally, we have recently observed both early (30–150 msec after sound onset)- and late (300–500 msec)-lateralized ERP responses to sounds in depth electrode recordings from low-level pericalcarine visual cortex (putative V1/V2) in two human patients with epilepsy (Brang et al., 2015). Thus, the putative mechanisms subserving crossmodal facilitations based on spatial versus temporal correspondences may not be as clearly dissociable as the literature exploring these phenomena independently appears to suggest.

To examine the relationship between these two putative mechanisms more closely, we used subdural and stereotactic electrocorticographic (ECoG) recordings from patients with epilepsy to examine the topography and timing of crossmodal phase resetting, bilaterally averaged ERPs, and ERP laterality differences evoked by sounds in visual cortex. Consistent with our previous research using centrally presented sounds (Brang et al., under review), lateralized noise bursts produced widespread phase resetting throughout visually responsive cortex, including pericalcarine, lateral occipital, inferior occipital–temporal, and posterior parietal cortex, with maximal activity in an occipitotemporal region potentially corresponding to area V5/hMT+. Averaging across contralateral and ipsilateral sound conditions, ERP responses showed a similar topography as the phase-resetting response, suggesting that the bilaterally averaged ERP response and crossmodal phase resetting likely reflect the same crossmodal activity.

To evaluate the relationship between this average bilateral response and laterality differences in crossmodal responses to sounds, we compared the cortical topography, magnitude, and time course of ERPs produced by contralaterally and ipsilaterally presented sounds in visual cortex. Laterality effects first emerged in pericalcarine and lateral occipitotemporal regions (50–150 msec) and spread to inferior occipitotemporal and posterior parietal regions over longer durations (150–400 msec), mirroring the topography of the phase reset and bilaterally averaged ERP responses. The majority of electrodes exhibiting lateralized responses produced significant responses to sounds in both hemifields, and no distinct region that consistently responded exclusively to either hemifield could be identified. Additionally, in participants with widespread coverage over visual cortex, the size of ipsilateral and contralateral responses were highly correlated across electrodes during both early and late response periods, but with a contralateral bias.

Together, these results suggest that crossmodal phase resetting, bilateral ERPs, and ERP laterality effects observed in response to sounds are generated by the same neural populations in visual cortex and, therefore, that a common mechanism may facilitate visual perception on the basis of spatial and temporal correspondences with sounds. Response laterality does not appear to arise from a distinct neural generator that responds exclusively to contralateral sounds but from a contralateral bias in neural populations that respond to sounds in visual cortex more generally. This result is consistent with a model of crossmodal interactions in which the properties of auditory cortical responses to sounds, including response laterality, are inherited by visual cortex, without the aid of an additional mechanism specialized for crossmodal conveyance of spatial information.

METHODS

Participants

Twenty-two patients with epilepsy participated in this study during invasive work-up for medically intractable
seizures using ECoG monitoring from chronically implanted depth electrodes (5 mm center-to-center spacing, 2 mm diameter) and/or subdural electrodes (10 mm center-to-center spacing, 3 mm diameter). Participants ranged in age from 15 to 56 (mean = 34.2, SD = 12.6) and included eight females. Electrodes were placed according to the clinical needs of the participants. Written consent was obtained from each participant according to the direction of the institutional review boards at the University of Michigan, University of Chicago, and Henry Ford Hospitals.

MRI and CT Acquisition and Processing

A preoperative T1-weighted MRI and a postoperative CT scan were acquired for each participant to aid in localization of electrodes. Cortical reconstruction and volumetric segmentation of each participant's MRI was performed with the Freesurfer image analysis suite (surfer.nmr.mgh.harvard.edu; Dale, Fischl, & Sereno, 1999; Fischl, Sereno, & Dale, 1999). Postoperative CT scans were registered to the T1-weighted MRI through SPM, and electrodes were localized along the Freesurfer cortical surface using customized open-source software developed in our laboratories (Brang, Dai, Zheng, & Towle, 2016; available for download online https://github.com/towel-lab/electrode-registration-app/). This software segments electrodes from the CT by intensity values and projects the normal tangent of each electrode to the dura surface, avoiding sulcal placements and correcting for postimplantation brain deformation present in CT images.

Lateralized Sounds Paradigm

Participants were seated in a hospital bed. Auditory stimuli were delivered via a laptop using PsychToolbox (Brainard, 1997; Pelli, 1997) through a pair of free-field speakers placed approximately 45° to the right and left of participants’ midline. The laptop and speakers were placed on a mobile overbed table, producing a viewing distance of approximately 80 cm. Two variants of the task were utilized across participants. Data were combined across tasks because previous studies have demonstrated similar crossmodal responses in both tasks (Feng et al., 2014; McDonald et al., 2013) and because we observed highly similar crossmodal responses in patients who completed both tasks. In Task A, participants were presented with one of three sounds on each trial: a 53-msec 1000-Hz sinewave tone presented from both speakers simultaneously and thus localized centrally (15 trials/block) or a 83-msec pink noise burst presented from either the left (30 trials/block) or right speaker (30 trials/block). Participants completed between two and six blocks. Stimuli were selected for consistency with the paradigm used by McDonald et al. (2013; Experiment 4). A central fixation cross was displayed on the laptop throughout the experiment. Participants were instructed to maintain central fixation and to respond via button press to the central 1000-Hz tone while making no response to the peripheral noise bursts (for which ECoG responses were analyzed). The ISI varied randomly between 2.0 and 2.5 sec (uniform distribution). Task B was based on the task used by Feng et al. (2014). The same 83-msec pink noise burst used in Task A was presented from either the left (60 trials/block) or right speaker (60 trials/block), with no central tone trials. At 400 msec after the presentation of a sound, a 50-msec duration visual letter (L or T) was presented on either the left or right side of the screen, followed by a 100-msec visual masking stimulus; sounds were not statistically predictive of the location of the subsequent visual target. Participants were instructed to identify the L or T stimulus via button press. The inter-trial interval varied randomly between 1.65 and 2.25 sec (uniform distribution). Participants completed between two and four blocks. Data from the visual portion of the trial were not examined for the purpose of this study, and analyses were restricted to the time period before their onset. Six participants completed Task A only, 11 completed Task B only, and 5 completed both.

ECoG Recordings and Analysis

ECoG recordings were acquired at 1024 Hz (14 participants), 4096 Hz (5 participants), or 1000 Hz (3 participants) due to differences in the clinical amplifiers used. Data recorded at 4096 Hz were down-sampled to 1024 Hz during the initial stages of processing. The onset of each trial was denoted online by a voltage-isolated TTL pulse. To ensure that electrodes reflected maximally local and independent activity from one another, we used bipolar referencing. Noisy channels, defined as those containing epileptic spiking (manually identified) or with an overall variance exceeding 5 SDs, were removed from analyses. Similarly, noisy trials, defined as those with an overall variance exceeding 3 SDs, were removed from analyses. These values were selected to match those used in our previous research using centrally presented sounds (Brang et al., under review). These values are the default used by our group and are based on the approach used by other groups as well (e.g., Jiang et al., 2017; Jacques et al., 2016), with values typically ranging from 3 to 5 SDs for both channel and trial rejection. Across both tasks, 4.7% (SD = 3.3%) of trials were rejected on average, resulting in the analysis of between 112 and 656 trials across participants (M = 252.0 trials per participant, SD = 151.9). Following the rejection of artifactual channels and trials, data were high-pass filtered at 0.01 Hz to remove slow drift artifacts and notch-filtered at 60 Hz and its harmonics to remove line noise. Data were then segmented into 4-sec duration epochs (−2 to 2 sec around the onset of the sound).

Specific analyses applied are described in-line throughout the Results section. In general, data were subjected to measures of the ERP in which the raw voltage time
series from each trial are averaged across trials in a time-locked manner. ERP data were baselined relative to the 500 msec before sound onset (prestimulus period ranging from −500 to 0 msec). Two-tailed one-sample $t$ tests were used to examine whether single ERP conditions differed from zero at any time point following sound onset. To control for statistical tests conducted at multiple time points, multiple comparison corrections were applied at each channel using maximum statistics (Holmes, Blair, Watson, & Ford, 1996). In specific, a distribution containing 10,000 permuted values from the data (using either condition label swapping for two-sample $t$ tests or sign swapping for one-sample $t$ tests) were generated for each electrode and time point. Next, a $t$ test (either one-sample or two-sample depending on the comparison) was then conducted at each time point, and the maximum $t$ value for each electrode was taken from each permutation, resulting in a null distribution of 10,000 $t$ values for each electrode. Finally, the upper and lower 2.5% of this null distribution were taken as critical $t$ values; only $t$ values in the real data exceeding these thresholds were considered statistically significant. Critically, this test controls the family-wise error rate at $p = .05$, indicating that purely random data would survive this multiple comparison correction at a rate of 5%. To control for statistical tests being applied across many channels and participants, the minimum multiple-comparison corrected $p$ value from each electrode was then false discovery rate (FDR)-corrected ($q = .05$) across all electrodes and participants (Groppe, Urbach, & Kutas, 2011).

Intertrial phase clustering (ITPC) analyses reflect the consistency of intrinsic oscillatory phase angles across trials, providing a general index of phase resetting. ITPC values were computed using nine wavelets (center frequencies ranging from 4 to 20 Hz at 2-Hz intervals, using a 750-msec Gaussian temporal window at each frequency). Instantaneous phase angles were calculated at each time point, frequency bin, and trial from the resultant wavelet convolutions. ITPC values were calculated at each time point and frequency as the magnitude of the complex average of the phase angle vectors across trials between 0 and 250 msec following sound onset; this restricted time period was used to avoid temporal smoothing past 400 msec—the time at which a visual stimulus was presented in Task B. Values were then averaged over the 250-msec time period and across all frequencies yielding a single value for each condition/electrode indexing stable phase locking. ITPC values are bound between 0 (uniform phase angle distribution) and 1 (identical phase angles across trials). To identify significant ITPC values for each electrode, a null distribution (10,000 permutations) was constructed from phase-shuffling the angle of filtered data before the calculation of ITPC values. In specific, a random value ranging from $-\pi$ to $+\pi$ (uniformly sampled) was added to each trial before calculation of ITPC in each permutation iteration. Critically, on each permutation, only a single random phase offset was applied to all time points and frequencies to maintain spectrototemporal dependencies in the data. To evaluate the statistical reliability of ECoG phase resetting, we computed the difference in ITPC values between the real stimulus-related data and data obtained from each permutation in the null distribution, counting the number of permutations with ITPC values exceeding those of the real data; electrodes at which <5% of the permuted ITPC values exceeded the real ITPC values were considered statistically significant. As in the ERP analyses, this method controls the family-wise error rate at 5%. FDR multiple comparison corrections ($q = .05$) were then applied across all electrodes and participants.

**Selection of Visual Electrodes**

Electrodes included for analyses are displayed in Figure 1. Visual electrodes were limited to those located in occipital, parietal, or temporal areas (excluding the superior temporal gyrus) and showing a significant ERP ($p < .05$, multiple comparison corrected) to visual stimuli beginning at less than 200 msec using a separate visual localizer task that presented participants with complex visual stimuli (e.g., faces, objects, scenes). All electrodes were projected onto the left hemisphere of an MNI-152 brain for visualization.

**RESULTS**

Previous research has identified two potential mechanisms for auditory facilitation of visual cortical processing: Whereas crossmodal phase resetting is thought to underlie enhancements based on audiovisual temporal correspondences (Thorne & Debener, 2014), interhemispheric differences in occipital ERPs are thought to reflect enhancements based on audiovisual spatial correspondences (Hillyard et al., 2016). However, the relationship between these putatively distinct effects is unclear. To clarify whether these effects reflect related or distinct processes, we leveraged the excellent spatial resolution provided by densely sampled intracranial recordings to compare the cortical topographies and time courses of crossmodal phase resetting, bilaterally averaged ERPs, and ERP laterality differences observed in response to sounds in visual cortex. Averaging across contralateral and ipsilateral sound conditions, we first tested whether bilaterally averaged ERP responses to sounds exhibited a similar neural topography as the auditory phase reset response in visual cortex. Then, we performed multiple tests to evaluate whether this bilaterally averaged response and lateralized ERP differences were generated by distinct neural populations that separately encoded spatial and nonspatial stimulus information or reflected a common laterality-biased response from the same neural generators.
Comparison of Crossmodal Phase Reset Responses and Auditory-Evoked Visual ERPs

Because event-driven phase resetting can generate ERPs (Klimesch, Sauseng, Hanslmayr, Gruber, & Freunberger, 2007; Sauseng et al., 2007), we first tested to see whether the overall ERP response to sounds, averaged across contralateral and ipsilateral conditions, could plausibly be attributed to crossmodal phase resetting. To test the hypothesis that the bilaterally averaged ERP response was produced by the same neural generators as the crossmodal phase reset response in visual cortex, we compared the spatial distributions of visual electrodes that displayed ERPs to the spatial distribution of those that displayed significant phase clustering (ITPC) in response to lateralized sounds. Both analyses were performed by pooling ipsilateral and contralateral responses and therefore reflected the nonlateralized component of the crossmodal response to lateralized sounds.

Consistent with our previous research using centralized sounds (Brang et al., under review), lateralized noise bursts produced widespread phase clustering throughout visually responsive cortex, indicating widespread crossmodal phase resetting distributed across multiple visual regions (Figure 2A). Altogether, 153 of 313 (48.9%) visual electrodes showed significant ITPC during the 250 msec following sound onset. Significant electrodes were observed in pericalcarine, lateral occipital, inferior occipital–temporal, and posterior parietal cortex, with maximal activity in an occipitotemporal region posterior to the middle temporal gyrus. The anatomical location of this latter area was consistent with the expected location of visual area V5/hMT+, though we could not verify the functional specificity of this area using motion-based localizers. The close correspondence between the cortical topography of this response and that previously observed to centralized sounds suggests that salient sounds produce widespread phase resetting throughout visual cortex regardless of stimulus location.

ERP responses to the same stimuli displayed a highly similar cortical topography (Figure 2B), suggesting that the average ERP response and crossmodal phase reset response likely reflect the same neural process. One hundred ninety-five of 313 (62.3%) of visual electrodes showed significant ERPs within 400 msec of sound onset. As in the phase clustering analysis, widespread auditory-driven ERPs were observed throughout visually responsive cortex, with close correspondences between the most active regions observed in each analysis. These results suggest that at least the nonlateralized aspects of crossmodal ERPs elicited by spatialized sounds likely reflect the same underlying process as the crossmodal phase reset response typically observed in nonspatial auditory tasks. However, this does not rule out the possibility of a separate neural population that responds exclusively to sounds in one hemifield, thereby providing an independent mechanism for enhancements based on spatial correspondence. To assess the possibility of such a mechanism, we compared the time course and

Figure 1. (A) Intracranial electrodes from 22 patients, displayed on an average brain (all electrodes projected into the left hemisphere). Each black or colored circle reflects a single electrode contact included in analyses, localized to visual areas (313 electrodes included in total). Electrodes were restricted to those located in occipital, parietal, or inferior/posterior temporal areas (excluding the superior temporal gyrus) and showing a significant ERP to visual stimuli beginning at less than 200 msec. Color-coded electrodes correspond to data in panel B and Figures 4 and 5. (B) ERP responses from representative electrodes evoked during visual task. Electrode numbers are located in the top left of each panel and correspond to the same numbers in Figures 4 and 5. Visual stimulus onset is at 0 sec (vertical dotted line). Shaded error bars reflect 95% confidence intervals.
Figure 2. Colored electrodes reflect significant (multiple comparison corrected for time points and electrodes) activity according to either (A) ITPC or (B) ERP analyses. Sounds activate visual cortex broadly and in a similarly distributed manner across both analyses, suggesting ERP and ITPC measures reflect similar mechanisms. The second row of images in each section reflects the same data on partially transparent brains to show statistics from electrodes not visible at the surface of the brain. The third row shows data from the individual electrodes shown in Figure 1B.
Figure 3. Colored electrodes reflect significant (multiple comparison corrected for time points and electrodes) differences between contralateral and ipsilateral sounds from either (A) 0–400 msec, (B) 50–150 msec, or (C) 150–400 msec. (B, C) Black electrodes reflect nonsignificant differences in one of the two time periods. The second row of images in each section reflects the same data on partially transparent brains to show statistics from electrodes not visible at the surface of the brain.
topographies of bilaterally averaged ERP responses and ERP laterality differences to assess whether they revealed two distinct regions that produced nonlateralized (i.e., spatially uninformative) and lateralized (i.e., spatially informative) responses to sounds.

**Identifying the Source of Response Lateralization in Auditory-Evoked Visual ERPs**

If response laterality associated with crossmodal spatial facilitation and nonlateralized responses associated with temporal facilitation through phase resetting reflect distinct neural mechanisms, then they would be expected to arise from distinct neural generators. By contrast, if lateralized and nonlateralized components of visual cortex’s response to sounds reflect two aspects of the same spatially biased response, they should arise from a common neural generator displaying a laterality bias.

To test the hypothesis that these two components arise from the same underlying mechanism, we compared them in a series of tests evaluating their topographies, magnitudes, and time courses. First, we compared the cortical topography of electrodes exhibiting bilaterally averaged ERP responses to the topography of those exhibiting laterality differences between contralateral and ipsilateral stimulus conditions. Overall, lateralized ERP differences were less widespread than bilaterally averaged responses, with 34 of 313 electrodes (10.9%) showing significantly different responses to contralateral compared with ipsilateral sounds (Figure 3A). This topographical difference may reflect the smaller effect sizes of the laterality differences relative to the average nonlateralized response, as observed in scalp EEG (e.g., McDonald et al., 2013), but likely also reflects decreased statistical power due to the division of trials into two conditions. Still, sites displaying significant laterality effects clustered...
closely around the lateral occipitotemporal, posterior parietal, and inferior occipitotemporal regions that showed the strongest nonlateralized component in our previous analysis, suggesting the possibility of a common neural generator.

Because previous studies using scalp-recorded EEG have shown temporally distinct “early” (50–150 msec) and “late” (150–400 msec) laterality effects, we also analyzed the topography of laterality differences during these two periods separately. Responses during the early period clustered around pericalcarine cortex and the lateral occipitotemporal region (potentially corresponding to area V5/hMT+) that showed the strongest effects in our analysis of the averaged bilateral response (Figure 3B), suggesting that the visual cortical response to sounds may originate from these sites. Responses during the late period included this region as well, with additional activity in dorsal (posterior parietal) and ventral (inferior occipitotemporal) sites, suggesting a pattern of spreading activation throughout visual cortex.

Although these results suggest a general spatial correspondence between the neural generators of laterality differences and the average bilateral response, their relationship can be evaluated more directly by testing whether electrodes showing a laterality effect respond exclusively to sounds in one hemifield or respond to both contralateral and ipsilateral sounds with a laterality bias. If laterality effects are produced by a distinct neural

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**Figure 5.** Locations of electrodes (red) corresponding to ERPs shown in Figure 4, highlighting areas at which significant differences between ipsilateral and contralateral ERPs were observed.
generator, then most electrodes displaying laterality effects should respond exclusively to sounds presented to one side. By contrast, if laterality effects result from laterality biases in the neural generators that produce the average bilateral response, then most electrodes showing laterality effects should respond to both contralateral and ipsilateral sounds, but with a spatial bias. Consistent with our hypothesis, the majority of electrodes displaying laterality effects (26 of 34, 76.5%) responded to both contralateral and ipsilateral sounds, but with a laterality bias (Figure 4); 6 of 34 (17.6%) only showed significant ERP responses to contralateral sounds; and 2 of 34 (5.9%) only showed significant ERP responses to ipsilateral sounds. Figure 5 shows the location of each individual electrode.

Whereas this analysis indicates that most electrodes displaying a lateralized response responded to both contralateral and ipsilateral sounds, it does not rule out the possibility of there being a small region in visual cortex that responds selectively to sounds presented only to a particular side. To evaluate this possibility, we visualized the locations of electrodes that displayed significant ERPs to contralateral, ipsilateral, or both types of sounds (Figure 6). Qualitatively, we could not identify any region displaying consistent selectivity for either contralateral or ipsilateral sounds. Rather, each major region identified in our previous analyses displayed mostly bilateral responses intermixed with spatially dispersed laterality-selective responses.

To evaluate this result in a more quantitative manner, we compared the effect sizes (Cohen’s d) of ERPs produced by contralateral and ipsilateral sounds across all electrodes present in four individual participants’ brains. These participants were selected because they each had at least 19 implanted electrodes, providing at least 80% power to detect correlations with coefficient \( r = 0.6 \), with a Type I error rate of \( \alpha = 0.05 \). Electrode locations for each participant are shown in Figure 7A.

If lateralized and nonlateralized aspects of crossmodal ERPs arise from a common neural generator with a laterality bias, then effect sizes for contralateral and ipsilateral sounds should be positively correlated across electrodes. By contrast, if there are distinct neural populations that respond selectively to sounds on a particular side, effect sizes should be negatively correlated or uncorrelated across electrodes. Notably, this analysis allows for a more fine-grained comparison of contralateral and ipsilateral responses than the previous analyses showing a similar distribution of significant electrodes, because it does not involve statistical thresholding before comparison. Cohen’s d values were calculated at each time point separately for contralateral and ipsilateral conditions by dividing the absolute value of the mean voltage at each time point by the standard deviation (across trials) of the voltage at the same time point. Absolute values were used because the directions of voltage deflections can vary with the position of electrodes relative to recorded activity, so effect magnitude is of primary interest. Using signed effect sizes produced larger correlation values, potentially reflecting inflated estimates produced by directional consistency within electrodes (i.e., correlations were exaggerated by consistency in the sign, rather than the magnitude, of effects across conditions).

The largest Cohen’s d value observed between 0 and 400 msec post-sound onset was extracted for each condition, yielding two values for each electrode. In all four

Figure 6. Electrodes showing significant ERPs during contralateral sounds (blue), ipsilateral sounds (orange), or both (purple). A majority of electrodes were significant in both analyses, suggesting similar neural mechanisms.
participants, we found strong positive correlations between the effect sizes of contralateral and ipsilateral ERPs, indicating predominantly bilateral responses across electrodes (Figure 7B). For all four participants, estimated regression slopes were less than one, with 95% confidence intervals excluding one (Participant 8: slope = 0.45, 95% CI [0.22, 0.68]; Participant 10: slope = 0.55, 95% CI [0.36, 0.74]; Participant 13: slope = 0.45 95% CI [0.37, 0.52]; Participant 15: slope = 0.66, 95% CI [0.54, 0.79]), suggesting a significant contralateral bias across electrodes. This result remained when intercept terms were fixed at zero. No significant correlations were observed when performing the same analysis on the prestimulus baseline period (Participant 8: $r(34) = 0.09, p = .61$; Participant 10: $r(27) = -0.08, p = .68$; Participant 13: $r(105) = 0.002, p = .98$; Participant 15: $r(17) = 0.13, p = .59$), indicating that correlations were driven by the poststimulus response, and not general differences in electrode sensitivity. Together, these results strongly suggest that lateralized and nonlateralized components of the visual cortical response to sounds arise from common neural generators that display a contralateral bias in their responses.

Because the timing of peak effect sizes varied considerably across electrodes and participants, including both early and late time periods identified in previous
research, we examined effect size correlations in a time-resolved manner to assess the time course of observed correlations throughout the entire analysis window (0–400 msec). For each participant, we computed correlations between contralateral and ipsilateral effect sizes for each electrode at each millisecond of the 400 msec response window (Figure 7C). Statistical significance was evaluated using FDR correction (q = .05) across all participants and time points. For all four participants, we observed significant correlations during both early (approximately 50–150 msec) and later (approximately 150–400 msec) periods emphasized in previous research. Because three of four participants (Participants 10, 13, and 15) exhibited temporally distinct peaks in their correlation time courses that corresponded approximately to previously identified “early” and “late” response periods, we examined the slopes of regression fits during these periods to test for contralaterally biased responses.

At time points corresponding to early peaks in the correlation time courses (Participant 8: 99 msec; Participant 10: 117 msec; Participant 13: 130 msec; Participant 15: 59 msec), each regression yielded a slope significantly (three of four) or nearly significantly (one of four) less than 1 (Participant 8: 0.66 [0.33, 1.01]; Participant 10: 0.73 [0.58, 0.87]; Participant 13: 0.57 [0.51, 0.64]; Participant 15: 0.66 [0.40, 0.93]), suggesting the presence of contralaterally biased responses during this period. At time points corresponding to later peaks (Participant 8: 295 msec; Participant 10: 319 msec; Participant 13: 315 msec; Participant 15: 371 msec), three of four regression slopes were significantly less than 1 (Participant 8: 0.60 [0.33, 0.87]; Participant 10: 0.77 [0.33, 1.22]; Participant 13: 0.40 [0.24, 0.56]; Participant 15: 0.51 [0.07, 0.56]), with all slope estimates being numerically less than 1, again suggesting contralaterally biased responses during this period. These results further reinforce the conclusion that the effects observed in separate analyses of laterality effects and bilaterally averaged responses do not reflect distinct lateralized and nonlateralized response but, rather, a single contralaterally biased response.

**DISCUSSION**

Co-occurring sounds can facilitate the perception of spatially (Lu et al., 2009; Driver & Spence, 2004; McDonald et al., 2000; Spence & Driver, 1997) or temporally (Chen et al., 2011; Fiebelkorn, Foxe, Butler, Mercier, et al., 2011; Jaekl & Soto-Faraco, 2010; Noesselt et al., 2010; Shams et al., 2002; Shipley, 1964) correspondent visual events. Separate lines of research have previously identified two putatively distinct neural mechanisms thought to underlie crossmodal facilitations based on each type of audiovisual correspondence. On the one hand, auditory-driven phase resetting is thought to facilitate the perception of simultaneous visual stimuli by placing visual cortex in a high-excitability state before visual signals arrive (Thorne & Debener, 2014). On the other hand, lateralized ERPs elicited by spatialized sounds are thought to facilitate the perception of spatially correspondent visual stimuli through hemisphere-specific excitation (or suppression) of visual cortex (Hillyard et al., 2016). Here, we sought to compare the topography and time course of these effects to examine the relationship between crossmodal enhancements associated with spatial and temporal correspondences.

Toward this end, we used densely sampled ECoG recordings from visual cortex to compare the neural generators of the auditory-driven phase reset response to those of the lateralized and nonlateralized aspects of the auditory-driven ERP response in visual cortex. We found that the topography of the bilaterally averaged ERP response closely matched the topography of the phase-resetting response produced by lateralized sounds in this study and centralized sounds in a previous study (Brang et al., under review), suggesting that both effects reflect the same underlying process.

To test whether this response reflected a distinct nonlateralized response that is mechanistically independent from the lateralized ERP differences produced by sounds in visual cortex, we performed three further analyses. First, we compared the cortical topographies of electrodes exhibiting bilaterally averaged ERP responses to those exhibiting laterality differences in response to contralateral and ipsilateral sounds. Although laterality differences showed a less widespread topography than bilaterally averaged effects, areas displaying significant laterality effects corresponded closely with those that showed the strongest bilaterally averaged response, suggesting a common neural generator.

Next, to determine whether response laterality was attributable to a distinct neural generator that responded exclusively to sounds in one hemifield, we tested whether individual electrodes displaying laterality effects responded selectively to sounds in either hemifield or responded to both sounds with a laterality bias. The majority of electrodes showed bilateral responses with a laterality bias, suggesting that laterality effects do not arise from a distinct neural generator but actually reflect laterality biases in the same neural responses that produce the nonlateralized component of the ERP response. No distinct subregion that responded exclusively to sounds in either hemifield could be identified.

Finally, to broadly characterize the lateralization of auditory responses in neural populations throughout visual cortex, we examined the relationship between the effect sizes of ERPs produced by contralateral and ipsilateral sounds across individual visual electrodes. In four patients with widespread visual coverage, we found strong positive correlations between the effect sizes of contralateral and ipsilateral ERPs, indicating predominantly bilateral responses across electrodes. The slopes of associated linear regressions revealed a contralateral bias across electrodes, suggesting that lateralized and
nonlateralized aspects of the visual cortical response to sounds arise from common neural generators that display a contralateral bias.

Taken together, these results suggest that crossmodal phase resetting and lateralized ERP effects, typically studied as distinct responses reflecting separate mechanisms for crossmodal facilitation, may actually arise from the same neural generators and, therefore, reflect the same underlying process. This result is consistent with a model of crossmodal facilitation in which lateralized responses to sounds in visual cortex are not produced by a distinct mechanism specialized for crossmodal conveyance of spatial information, but a laterality bias inherited from auditory cortex and possibly modulated through attentive mechanisms.

On this account, the properties of visual cortical responses to sounds do not arise from multiple specialized mechanisms responsible for the independent processing of various crossmodal correspondences, but rather from the passive carryover of the properties of the auditory cortical response to sounds—including response laterality—to visual cortex. As auditory cortex shows a contralateral bias in its response to sounds (e.g., right auditory cortex responds more strongly, but not exclusively, to left lateralized sounds; Kaiser & Lutzenberger, 2001; Celesia, 1976) and is thought to possess anatomical connections to visual cortex in the same hemisphere (right auditory cortex is connected to right visual cortex; Rockland & Ojima, 2003; Falchier, Clavagnier, Barone, & Kennedy, 2002), auditory cortex's laterality bias may be passively carried-over to connected visual areas in the same hemisphere, resulting in a laterality bias in visual cortical responses to sounds.

One primary advantage of this explanation is that it can simultaneously account for the seemingly contradictory findings of context- or task-contingent laterality effects in visual cortical responses to sounds, which have been taken to suggest a distinct mechanism for spatial interactions across the senses, and our current results, which suggest the absence of such a mechanism. Previous studies suggest that laterality effects in occipital responses to sounds may depend on the task relevance (Campus et al., 2017) and unpredictability (Matusz et al., 2016) of the locations of auditory stimuli. Because auditory spatial attention enhances response lateralization in auditory cortex (Alho et al., 1999; Teder-Sälejärvi, Hillyard, Röder, & Neville, 1999), the results of these attentional modulations may also be transmitted to visual cortex, producing larger lateralization effects when auditory spatial information is task relevant (drawing endogenous auditory spatial attention; e.g., Campus et al., 2017) or unpredictable (drawing exogenous auditory spatial attention; e.g., Matusz et al., 2016). Thus, on this account, previously observed modulations of crossmodal laterality effects could reflect enhanced lateralization in auditory cortex due to auditory spatial attention, rather than a distinct multisensory mechanism that specifically conveys

auditory spatial information to visual cortex. Thus, we predict that manipulations of auditory spatial attention or spatial unpredictability would enhance the spatial biases observed in the current study but would not produce purely laterality-selective responses.

Although our results provide initial evidence consistent with such an account, further research is needed to verify the additional premises underlying the proposed model, which presupposes that visual cortex's response to sounds is inherited from auditory cortex. However, it is also possible that auditory information is transmitted to visual cortex by subcortical or thalamic pathways that would not display response laterality or attentional modulation (Cappe, Rouiller, & Barone, 2012). Although our previous research using amplitude-modulated sounds suggests that visual cortex's response to sounds mirrors the temporal dynamics of auditory cortical, but not subcortical, responses (Brang et al., under review), additional evidence is needed to confidently conclude that crossmodal responses in visual cortex originate from auditory cortex. Additionally, the proposed model rests on the assumption that auditory signals are transmitted to visual cortex via lateralized intrahemispheric connections between auditory and visual cortices. Although such connections have been observed in nonhuman primates (Rockland & Ojima, 2003; Falchier et al., 2002), it is currently unclear whether similar pathways exist in humans. Indeed, we have successfully reconstructed similar pathways using diffusion-weighted imaging (Plass, Zweig, Brang, Suzuki, & Grabowecky, 2015), though ambiguities regarding the accuracy of estimated cortical terminations in diffusion tractography currently preclude us from making conclusive claims regarding the presence or absence of this pathway in the human brain (Reveley et al., 2015). Therefore, although our results provide initial evidence for the proposed model, additional evidence is necessary to fully corroborate this account.

One specific prediction made by this model is that the lateralization of crossmodal responses to sounds in visual cortex should reflect the lateralization of auditory cortex's responses to sounds, including variations potentially produced by spatial expectation, attention, task demands, adaptation, trial-by-trial variability, and the eccentricity-dependent resolution of auditory spatial attention (e.g., Teder-Sälejärvi et al., 1999). Although the most stringent test of these predictions would be to compare activity in auditory and visual cortices throughout a variety of auditory tasks, electrode placements dictated by clinical needs rarely result in this type of extended coverage and no participant in the current study had such coverage. We are currently exploring alternative methods to test these predictions rigorously. An additional prediction is that the spatial specificity of auditory effects on visual perception should reflect the resolution of spatial information provided by auditory cortical laterality. For example, because auditory cortical responses are only partially
lateralized, auditory facilitations of visual perception should not be strictly hemifield specific and should occur even in cases of fairly coarse audiovisual spatial alignment. Behavioral and psychophysical studies are largely in agreement with this prediction, with auditory enhancements of visual detection and discrimination often proving to be surprisingly impervious to spatial misalignment (e.g., Spence, 2013; Fiebelkorn, Foxe, Butler, & Molholm, 2011).

One potential caveat to our interpretation is that, although we observed similar topographies across each of our analyses, it is still possible that distinct but closely collocated neural circuits or subpopulations separately generate the lateralized and nonlateralized responses observed in each area. For example, signals recorded by a single electrode may reflect the summed activity of neural populations in different cortical layers or adjacent patches of cortex. Still, given the high spatial precision provided by invasive intracranial electrodes, our results at least suggest that the generators of these responses are closely collocated and are unlikely to occupy distinct regions of visual cortex as previous research appears to suggest.

One additional concern is that the intracranially recorded responses analyzed here may not correspond precisely to crossmodal effects identified previously using scalp-recorded EEG (Matusz et al., 2016; Feng et al., 2014; McDonald et al., 2013; Naue et al., 2011) or TMS (Romei et al., 2012). Although additional research comparing source-localized EEG, TMS, and ECoG responses is needed to clarify the relationship between these effects more definitively, the response topography observed in this study is largely in agreement with previous results, with dominant effects in lateral occipital cortex corresponding approximately to EEG source localizations of laterality effects (Matusz et al., 2016; Feng et al., 2014; McDonald et al., 2013) and pericalcarine effects corresponding approximately to sites studied or stimulated in animal physiology (Lakatos et al., 2009). TMS (Romei et al., 2012), and human EEG studies of crossmodal phase resetting (Naue et al., 2011) and, arguably, some EEG studies of crossmodal laterality effects (Campus et al., 2017; Matusz et al., 2016; Feng et al., 2014).

Thus, the primary discrepancies between our results and (some) previous results are that we observe rapid lateralized responses in low-level visual cortex and laterality-biased responses at both “early” and “late” latencies. Because laterality effects were reliably smaller than the overall bilaterally averaged response, these discrepancies may simply reflect differences in sensitivity between ECoG and scalp-recorded EEG, potential weaknesses of EEG source localization (Bradley et al., 2016), and the fact that previous studies of phase resetting have tended not to consider response laterality. Additional activity in posterior parietal or occipitoparietal cortex may correspond to previously observed alpha activity associated with audiovisual spatial attention (Frey et al., 2014; Banerjee, Snyder, Molholm, & Foxe, 2011), but further research is needed to confirm this speculation.

Another potential concern is that patients’ inadvertent eye movements could have influenced observed cortical responses. Although eye movements were not rigorously monitored using eye tracking in this study, eye movements were monitored by the experimenter throughout the tasks and minimized through experimenter feedback. Previous studies using similar task protocols did not observe any eye deviations as measured by the EOG (McDonald et al., 2013), and our experimental observations, though less rigorous, were largely consistent with this result. Importantly, eye movements would not have been advantageous in either task because participants responded only to centralized sounds in Task A and the auditory cue location was not predictive of visual target location in Task B. Moreover, the early auditory-evoked responses observed in this study are unlikely to have been contaminated by eye movement-related activity because saccades to lateralized sounds typically take 150–300 msec to initiate (Gabriel, Munoz, & Bohnhke, 2010; Yao & Peck, 1997; Frens & Van Opstal, 1995) and saccade-induced neural responses in low-level visual cortex and area MT tend to occur 40–100 msec after saccade onset (e.g., Kagan, Gur, & Snodderly, 2008; Bair & O’keefe, 1998). Thus, saccade-related activity is unlikely to have contaminated the earlier responses observed in this study. Although later responses could have conceivably been contaminated by eye movements, these responses are largely consistent with previous source localizations of late-lateralized ERPs in scalp-recorded EEG during rigorous monitoring of eye movements and are therefore unlikely to reflect eye movement-related activity.

Finally, additional research is necessary to better characterize the visual or other functions of the cortical sites identified in this study. Although each of our analyses repeatedly pointed to a lateral occipitotemporal region, potentially corresponding to area V5/hMT+, as a critical site for audiovisual interactions, we were unable to verify the specific functional properties of this area using, for example, motion-based localizers. Further research is needed to verify whether this site indeed corresponds to motion-sensitive area V5/hMT+ or an adjacent site with distinct functional properties. Additionally, given the nature of our functional localizers, we cannot rule out the possibility that some sites identified in this study would be better characterized as multisensory association cortex than as visual cortex. More detailed characterization of the functional properties of each site is necessary to clarify this question; however, this distinction may rest more on semantic convention than on actual substance, given the widespread prevalence of multisensory interactions throughout neocortex (Ghazanfar & Schroeder, 2006). Altogether, our results suggest that auditory phase resetting of visual activity (responsible for relaying temporal information to the visual system) and lateralized ERP effects (responsible for relaying spatial information to the visual system) can be accounted for by a single neural mechanism.
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Reprint requests should be sent to David Brang, Department of Psychology, University of Michigan, 530 Church Street, Ann Arbor, MI 48109, or via e-mail: djbrang@umich.edu.

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